

Two-piece zirconia implant for global metal-free restoration

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Zirconia in dentistry has historically been known for its strength and biocompatibility characteristics in simple or complex prosthetic rehabilitation. Only in the last decade has it become more widely used in implantology as well. Zirconia is a mixture of composites based on zirconium dioxide. Zirconium is the metal from which the eponymous dioxide is derived. The powders used to obtain zirconia have a very high degree of purity and are obtained through complex chemical and co-precipitation procedures.¹ The crystalline structure of zirconia occurs in different geometric shapes depending on the temperature to which it is subjected and reversibly changes from a monoclinic state at room temperature to a tetragonal state up to 1,100 °C and a cubic state at around 2,400 °C. Therefore, the density of the material is determined by the shape and size of the geometric state, which determines a different final size and a different physical property, depending on the heat treatment.²

Sintering takes place at temperatures above 1,170 °C, determining a change of state from tetragonal to monoclinic. This causes stress that leads to fracture of the artefacts, which is why oxides were introduced to stabilise the composite and prevent fracture. In the medical field, various oxides, such as magnesium oxide, titanium dioxide, alumina, yttrium oxide and ceric oxide, are used in small percentages combined with zirconia, creating stability in various sintering processes and cre-

ating a family of zirconia-based ceramics with different chemical, physical and structural characteristics.³

Advancement in dental implantology occurred with the addition of yttrium oxide to zirconia, generating yttrium tetragonal zirconia polycrystals (Y-TZP). Although this achievement has only recently been translated to clinical practice, the initial studies date back to the early 1960s with ceramic materials that allowed such maturation and knowledge that today allow a degree of excellence for biomechanics and integrative biocompatibility with the hard and soft tissue of the oral cavity.⁴ Zirconia does not cause systemic or local cytotoxicity, and cytocompatibility *in vivo* and *in vitro* has been reported.⁵ In order to accelerate the healing time, osseointegrative properties were achieved through surface treatment by increasing hydrophilicity with different procedures.¹¹ Bacterial colonisation and adhesion to the implant surface are related to the material type used, Y-TZP having significant advantages over titanium.¹⁰ *In vitro* tests have shown less accumulation of the various bacterial strains present in the oral cavity, and significant results of less adhesion on zirconia or titanium abutments has been demonstrated *in vivo*.^{12–16} The absence of metal oxides allows for improved biological response of the gingival tissue, resulting in reduced bacterial formation and subsequent inflammatory onset.¹⁸

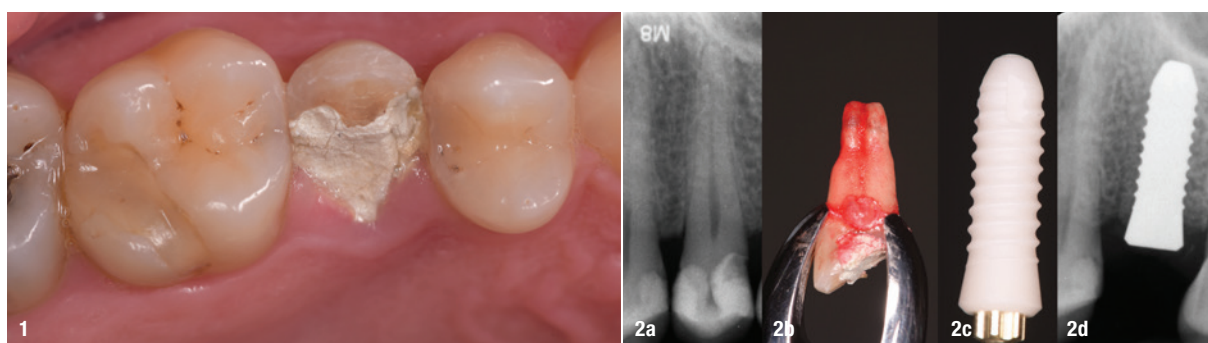


Fig. 1: Occlusal image of the coronal fracture of the partially medicated tooth to soothe the thermal sensitivity caused by uncovering of the pulp chamber. **Figs. 2a–d:** Initial radiographic image showing the close proximity to the floor of the maxillary sinus in addition to the viability of the tooth and the absence of periradicular infection (a). Extracted root (b). CERALOG Hexalobe implant (c). The result of implant placement with respect to the sinus floor and the osseous and interradicular relationship (d).



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Fig. 3: Occlusal view of the CERALOG implant placed using a flapless technique and filling of the spaces between the bone and implant. **Fig. 4:** Provisional PEEK abutment *in situ*, to which the provisional crown produced by CAD/CAM was to be bonded. **Fig. 5:** The tissue conditioning and bone healing situation after 56 days of functional loading with the provisional crown.

The characteristic white colour of zirconia implants blends in better below the gingival tissue, especially in thin phenotypes, avoiding those unsightly grey shadows peculiar to titanium implants, especially for those implant designs with a smooth collar. Moreover, even in the case of gingival recession, no exposure of metal portions occurs.¹⁷

An important aspect that characterised the first generation of zirconia implants was the frequency of fracture, being about 4%, especially in the first year of loading, in cases of particular tightening of the abutments with metal screws and in two-piece implants with a diameter of less than 3.5 mm.¹⁹ The rate has dropped below 0.5% owing to advancements in the manufacturing process, in material preparation and in implant fabrication whether by milling or isostatic pressing.²⁰

As an additional fact to be noted in the knowledge of this new implant material concerns the ageing of the structure, better known as hydrothermal degradation (low-temperature degradation), that occurs at temperatures above 150 °C in an environment with the presence of water.²¹ In order to fully control such degradation, ceric oxide or alumina was added to the zirconia powder composite.²² Based on the experience gained in these 30 years of research and development, we can now consider zirconia implants a viable substitute for titanium implants, especially in highly

aesthetic areas or in those patients in whom tissue quality or particular susceptibility to bacterial colonisation may require a greater guarantee of long-term outcome.^{23, 24}

Clinical case report

The male patient was a 53-year-old non-smoker in an excellent state of health, ASA I, with vertical fracture of the crown of tooth #25 associated with spontaneous pain. In the first phase of treatment, we conducted an accurate clinical and diagnostic diagnosis in which we ascertained the possible therapeutic variables aimed at coronal restoration after crown lengthening, root canal therapy and core reconstruction on which to finalise a clinical crown. The patient presented to the clinic with masticatory trauma that had caused a clear fracture of the palatal cusp of the vital tooth restored according to a direct composite technique. The fracture was extensive in depth to at least 1 mm subcrestally, in addition to uncovering the pulp chamber (Fig. 1). After careful evaluation and comparison of procedures, the patient was shown the various treatment options and opted to have the fractured tooth replaced with an implant. The choice of a ceramic implant was considered for a number of factors, including global metal-free restoration and an aesthetic outcome. We decided on a two-piece Y-TZP implant (CERALOG™, BioHorizons Camlog) made using a high-tech production process for molding (Ceramic Injection Molding–CIM).

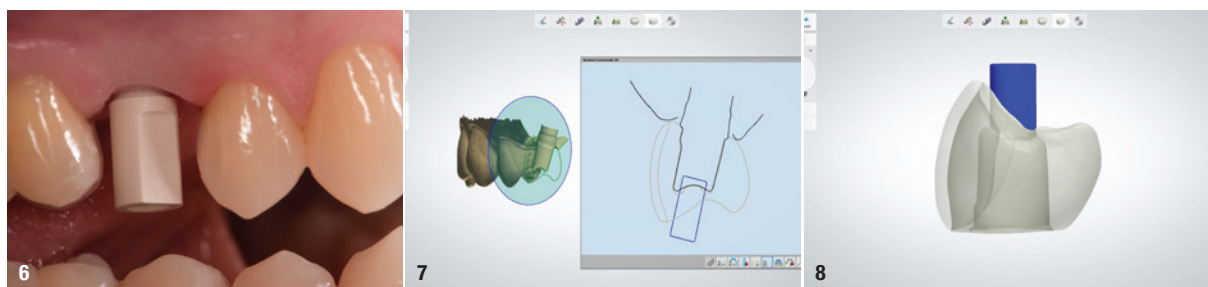


Fig. 6: The scan body on the implant. **Fig. 7:** The sectional design of the crown allowed for a broad evaluation. **Fig. 8:** The design showing subtraction from the vestibular aspect to accommodate the ceramic layering.

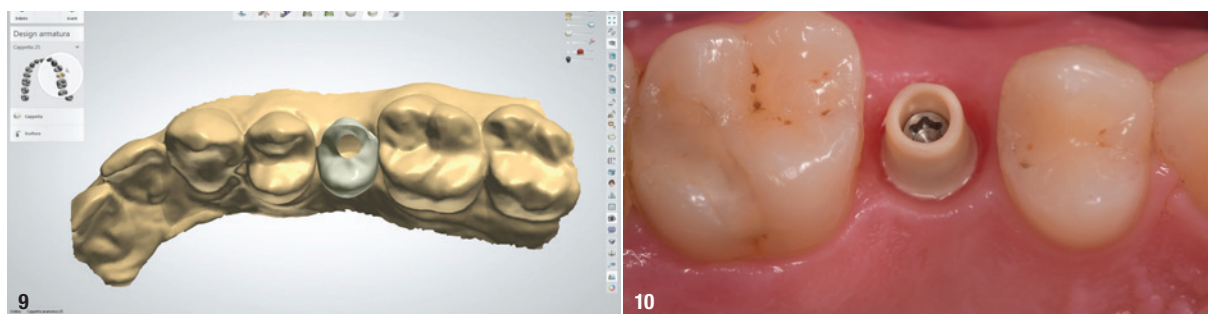


Fig. 9: View of the design in the context of the virtual model, showing the transition points in the adjacent contacts and the access hole in the occlusal aspect, avoiding compromise of aesthetics and of resistance to masticatory forces. **Fig. 10:** The final abutment of PEKK, a biocompatible material that is resistant to oral fluids and masticatory forces.

Root extraction was performed according to a flapless technique, avoiding injury to the cortical bone. The use of piezo-surgery allowed for facilitated removal without cortical compression (Fig. 2). Site preparation is a delicate step in implant surgery, especially for zirconia implants. In fact, ceramic implants tolerate screwing stresses poorly; therefore, the site must be carefully prepared with adequate irrigation and possible tapping of the site, especially in cases of Class D1 and D2 compact bone. In the present case, subcortical insertion was not necessary, but in the event of need, there is a countersinking function available in the CERALOG system, which allows placing the implant subcrestally while avoiding cortical compaction that usually induces vertical resorption.

Like with titanium implants, placement of zirconia implants requires primary stability. The difficulty is initially associated with the point of engagement of the first drill to match the centre of the implant with the inter-coronal distance. It is not always possible to use this point for implant insertion because of the variables associated with root shape and the number of roots present. The maxillary second premolar usually presents a single root or in some cases two fused roots, and therefore it lends itself more easily to a contextual replacement. The only problem is associated with the upper boundary with the cortical floor of the maxillary sinus that could limit the excursion of the pilot drill beyond the apex in search of greater primary stability (Fig. 2).

In this case, a cylindrical body zirconia two-piece implant of 12.0mm in length and 4.1mm diameter was used considering that the prosthetic collar had a diameter of 4.5mm. The spaces between the bone and the implant were filled with slowly resorbing biomaterial to better preserve the alveolar bone. The implant was deliberately not restored immediately, because although the primary stability achieved was 55 ISQ, we preferred to leave the implant to heal naturally and not expose it to further occlusal trauma (Fig. 3). A healing abutment was placed on the implant.

After eight weeks, we removed the healing abutment and took a digital impression for the preparation of a provisional restoration placed on a PEEK temporary abutment for an additional four weeks (Fig. 4), at the end of which we removed the screw-retained provisional crown and noted the degree of peri-implant mucosal conditioning. We took a new impression with an intra-oral scanner using a scan body (Figs. 5 & 6). By using the implant system's scan body, we were able to capture the implant's specifications or the dental technician. The scan body stops at the implant connection and does not interfere with the soft tissue. The digital impression also allows for excellent reading of the conditioned tissue so that the aesthetic margins achieved can be followed. The file was sent to the dental laboratory after filling out the attached data sheet listing the implant type and model, the type of restoration desired, whether screw-retained or cemented, and the material with which it was to be finalised. The software is able to detect colour values so that an initial colour indication can be defined.

The choice of a two-piece zirconia implant allows a single restoration or possibly a multi-unit cemented restoration thanks to the design of dedicated frameworks utilising CAD/CAM and the DEDICAM CAD libraries. The data collected is supported by photographic status and spectrophotometric images. Digital data has great versatility of use and limited cost and offers great potential for use and communication effectiveness even at a distance. The dental technician was able to make a careful assessment of the implant position, the possibility of making a screw-retained prosthesis, the aesthetic margins, and the prosthetic components to be used. The dental technician is able to determine the feasibility of the restoration according to the prescription, sharing with the clinician the potential and limitations present in the specifications. It is not always possible to have an angulated screw-retained abutment allowing an access hole in a region congruous with the aesthetics and function of the implant in case the implant-abutment connection is modified by inclining the bearing surface of the implant shoulder (Fig. 7).

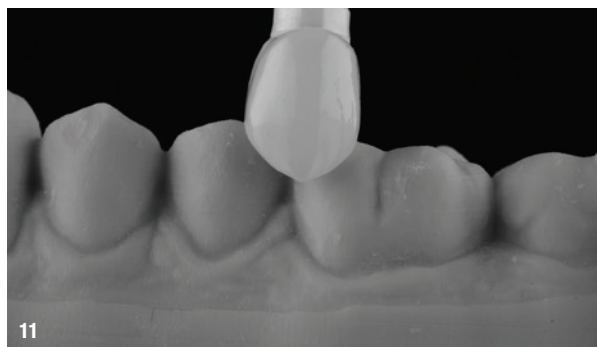


Fig. 11: View of the completed crown, the abutment to which it is bonded and the ceramic analogue. **Fig. 12:** Vestibular view three years after loading.

Given the special attention to the aesthetic component, we preferred to add ceramic to the coronal zirconia structure, maintaining a high-strength structure in the portion bordering the access hole and simultaneously enhancing the aesthetics with a portion characterised by ceramic layering and not simply coloured. Having established the prosthetic design and chosen the material, the design proceeded with subtraction from the vestibular aspect in the appropriate volume to accommodate the ceramic addition (Fig. 8). When deciding on a technical procedure for layering, it is crucial to have a model that can facilitate the dental technician in fabrication (Fig. 9). The abutment used for the definitive restoration is different from the one used for the provisional restoration, in material and shape. The portion of the abutment that seals the connection with the implant cannot be modified by either subtraction or addition, so the crown would be cemented in the laboratory to the abutment (Fig. 10). A removable transfer of both the implant and digital models would be housed on the model, enabling its specifications to be entered into the prosthetic design software. All this data that seems obvious in reality should be verified before taking and sending the impression to the laboratory (Fig. 11). Radiographically, the abutment appears as a space between the implant and the crown, being radiolucent.

Prosthetic placement was performed according to the manufacturer's instructions by dynamometric tightening with a Unigrip screwdriver to 15Ncm for Holisticor screws in gold or 25Ncm in titanium. The three-year follow-up found no signs of clinical concern, and the result was a functional implant restoration that appeared perfectly natural (Fig. 12).

Discussion

The particular conformation of the prosthetic connection (CERALOG™ Hexalobe) firmly stabilises the abutment to the implant, preventing unscrewing, even in the long term and even if tightening was not done with a torque wrench. The PEKK abutment comparing to a standard polymer abutment in PEEK has a higher ten-

sile strength and excellent thermoplastic performance, ensuring resistance to masticatory stress. It is possible to employ cemented or screw-retained crowns, depending on the type of rehabilitation and especially depending on the inclination of the implant and the aesthetic requirements of the prosthetic restoration.

Conclusion

The choice of a zirconia implant is now a well-established procedure especially in cases like this one where aesthetic requirements and the desire for metal-free treatment are combined. Tissue response is always positive, and its maturation improves over time by stabilising and improving the mucosal surface. Probably poor bacterial colonisation and adhesion is a significant factor in the absence of peri-implant inflammation, and this is an ideal prerequisite for progressive and evolutionary tissue maturation. Tissue response improves over time.

about the author



Dr Riccardo Scaringi teaches specialisation courses in dental implant prosthetics and digital support technologies at various universities in Italy. He is frequently invited to speak at national congresses on topics related to surgical prosthetics. He is also an active member at the most prestigious international scientific associations in the field of technological and digital surgery. Dr Scaringi is the author of various scientific texts.

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